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Anatomy to understand pelvic trauma: structure and function of several ligaments around the sacroiliac and pubic symphysis, and bone mineral density of the pelvic bones

Short title: Anatomy to understand pelvic trauma: pelvic ligaments and BMD

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Abstract

This review is based on the literature published between 2000 and 2023 and presents an up-to-date evidence-based discussion of anatomical considerations relevant to the management of pelvic trauma. In addition, it discusses the significance of the pelvic ligaments in stabilizing the pelvic ring and of bone mineral density (BMD) in fragility fracture of the pelvis (FFP), which is becoming increasingly common in today's aging societies. Following an overview of the anatomy and function of the sacroiliac joint (SIJ), the pubic symphysis, and the surrounding ligaments, the suitability of the widely used Young-Burgess classification of high-energy impact pelvic ring fractures, which emphasizes the role of the ligaments in pelvic ring injuries, is discussed. Based on the current body of knowledge, using 2.5 cm of pubic symphysis diastasis as the determinant for surgical intervention for anterior-posterior compression fracture is questioned, and evaluation under anesthesia and lateral stress radiography for accurate diagnosis and treatment planning is proposed instead. The review underscores the need for further research on how the pelvic ligaments can provide optimal stability in the treatment of various types of pelvic fracture. On the other hand, for fragility fracture of pelvis (FFP) in older adults caused by low-energy trauma, the emphasis is on the fragility of the bones. To better manage FFP, the importance of understanding the distribution of BMD in the pelvis is highlighted. Dual-energy X-ray absorptiometry is a common method for measuring BMD, but it has drawbacks. The advantages of measuring BMD using Hounsfield units on computed tomography scans as an alternative method are discussed. An understanding of these issues may lead to better

management of the increasing number of FFP cases in older people with reduced BMD.

和文抄録

題目: 骨盤外傷を理解するための解剖学;仙腸関節と恥骨結合の靭帯の構造と機能および

骨盤骨の骨密度

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抄録: 本稿では 2000 年から 2022 年までの文献レビューを基に骨盤外傷の管理と治療戦略における解剖学的考察と今日の高齢化社会で一般的となりつつある骨盤脆弱性骨折における骨盤骨の骨密度の重要性について述べる。初めに仙腸関節と恥骨結合およびその周囲の靭帯の解剖学とその機能について概説する。高エネルギー外傷による若年者の骨盤輪骨折について Young-Burgess 分類を使用して骨盤輪の損傷時における靭帯の役割を強調する。APC 型の骨盤輪骨折に対する治療の基準として恥骨結合離開が 2.5cm 以上とされる従来の考え方に疑問を呈した。代わりとして、麻酔下でのストレス撮影 (EUA) や自重を用いた X 線側面像 (LSR) を不安定性の正確な評価と治療の計画立案を提案する。一方で、低エネルギー外傷によって引き起こされる高齢者の脆弱性骨盤輪骨折に対しては骨が脆弱であることが強調される。脆弱性骨盤輪骨折をより良く管理するためには、骨盤骨の詳細な骨密度を理解することが重要であったが、一般的な検査方法である DEXA 法では評価が不十分であった。代わりとして CT scan での Hounsfield 単位 (HU) を用いた測定がなされて

いる。これらの結果は骨折型の理解や手術方法の立案に役立つ可能性が高い。

1 **Introduction**

2 Pelvic ring fractures may be caused by high-energy trauma, such as a road traffic accident, or by
3 fragility fracture of the pelvis (FFP) in response to low-energy trauma, such as a fall, in individuals
4 with reduced bone mineral density (BMD) ¹⁾. The bony anatomy of the pelvic ring, formed from the
5 sacrum and the two innominate bones, each with an ilium, ischium, and pubis, has no inherent
6 stability and needs strong ligamentous attachments to maintain the ring structure. Displacement
7 occurs when the ring is disrupted at two or more sites ²⁾. High-energy traumatic fractures of the
8 pelvic ring can be life-threatening and require immediate intervention ³⁾. The Young-Burgess
9 classification is widely used in the management of high-energy trauma fractures and classifies such
10 fractures according to bone and ligament failure. Therefore, a thorough understanding of the anatomy
11 and stabilizing function of the relevant ligaments is needed, especially those around the sacroiliac
12 joint (SIJ) and the pubic symphysis. This narrative review discusses the anatomy of these ligaments,
13 focusing on their role in stabilizing the pelvic ring during movement and their significance in terms
14 of the Young-Burgess classification of pelvic fractures.

15 Clinicians managing low-energy traumatic FFPs often have concerns about inadequate surgical
16 fixation; although the ligaments are intact, the bone tissue is fragile as a result of decreased BMD
17 and can fracture easily. In view of the increasing incidence of FFPs as a result of loss of BMD in
18 today's aging societies, this review discusses the most recent literature on pelvic BMD and the
19 methods used to measure it when planning treatment. The literature published between 2000 and

20 2023 was searched using the PubMed database.

21 **1 Sacroiliac joint**

22 **1.1 Bony anatomy**

23 The SIJ connects the spine to the pelvis and allows transfer of load between the lumbar spine and the
24 legs ¹⁾. Located within the pelvis between the sacrum and ilium, the SIJ is a diarthrodial synovial
25 joint ⁴⁾ with a width of 1–2 mm and is surrounded by a fibrous capsule that is attached to the sacrum
26 and ilium ⁵⁾. The dorsal area of the joint houses the fibrous interosseous sacroiliac ligament (ISL),
27 while the ventral area contains the L-shaped synovial articular cartilage. The sacral joint is covered
28 with approximately 1 mm of hyaline cartilage, which has a more fibrocartilaginous appearance. The
29 cortical bone is extremely thin and has a width of less than 1 mm ⁶⁾.

30 **1.2 Ligamentous anatomy of the SIJ**

31 **1.2.1 Anterior sacroiliac ligament**

32 As described in the excellent comprehensive review by Ashby et al. ⁷⁾, the anterior sacroiliac
33 ligament (ASL) is located on the anterior aspect of the SIJ ⁸⁾. It has long transverse fibers that run
34 from the sacral base and lateral sacrum to the medial margin of the auricular surface of the ilium. The
35 superior portion is an extension of the iliolumbar ligament (ILL). Caudally, it merges with the cranial
36 fibers of the sacrospinous ligament ⁹⁾. The fibers of the ASL are mainly thin and weaker than those of
37 the posterior sacroiliac ligament (PSL) ⁵⁾. However, the ASL is well developed where it runs over the
38 SIJ obliquely to connect the third sacral segment to the ilium near the arcuate line and the posterior

39 inferior iliac spine ^{7),8)}.

40 **1.2.2 Interosseous sacroiliac ligament**

41 The ISL is situated deep within the dorsal sacroiliac ligament, positioning itself between the ilium
42 and the sacrum. It has a unique, funnel-shaped architecture with the apex linked directly to the
43 sacrum. This ligament completely encapsulates the axial joint and occupies the dorsal and cranial
44 space within the synovial portion of the joint, thereby conferring considerable multidirectional
45 structural stability. Remarkably, the ISL has the most significant osseous origin and volume among
46 all the SIJ ligaments. The substantial structure and size of the ISL means it as the strongest of all the
47 ligaments supporting the SIJ, highlighting its pivotal role in maintaining the stability and
48 functionality of the joint ⁷⁾.

49 **1.2.3 Posterior sacroiliac ligament**

50 The PSL exhibits distinct proximal and distal zones of bony anchoring, with an intervening segment
51 housing a nexus of three layers: the erector spinae aponeurosis, the intricate deep fascial layer, and
52 the gluteal aponeurosis ⁷⁾. Short PSLs trace a path from the posterior tuberosity of the ilium,
53 culminating at the lateral facet of the sacrum. These ligaments, with their fibers primarily oriented
54 horizontally, contribute to the depth of the ligamentous complex ⁷⁾. Long PSLs, characterized by
55 considerable resilience, are constituted by several bundles of fibers. They span from the lateral crest
56 of the sacrum, reaching towards the posterior superior iliac spine and the terminal of the iliac crest ⁵⁾.
57 This strategic anatomical positioning affords a protective mechanism against potential posterior

58 flaring or joint diastasis ¹⁰).

59 **1.2.4 Iliolumbar ligament**

60 Originating from the transverse processes of L4 and L5 and extending to the iliac crest, the ILL is
61 attached to the pelvis via two primary bands reaching the sacroiliac capsule ⁸) and restricts sagittal
62 movement of the SIJ ¹¹).

63 **1.2.5 Sacrotuberous ligament**

64 The sacrotuberous ligament, with its vertical orientation and broad base that attaches to the posterior
65 superior iliac spine, the PSL, the lateral sacral crest, and the lateral margins of the lower
66 sacrum/upper coccyx, plays a critical role in the kinematic chain. It supports the direct transmission
67 of mechanical force and load from the spine and sacrum to the lower limbs ¹¹). Anchoring to the
68 medial margin of the ischial tuberosity, the sacrotuberous ligament contains superficial fibers that are
69 continuous with the biceps femoris tendon. Working in concert with the sacrospinous ligament, it
70 firmly secures the sacrum to the ischium, effectively preventing upward tilt ¹²).

71 **1.2.6 Sacrospinous ligament**

72 The sacrospinous ligament, which is characterized by a thin and triangular profile, occupies a
73 position posterior to the attachment of the sacrotuberous ligament. It forms a crucial connective link
74 from the outer margins of the sacrum and coccyx to the ischial spine of the ilium. Interestingly, this
75 ligament exhibits some blending with the sacrotuberous ligament, demonstrating the intricacy of this
76 ligamentous network ⁸).

77 **1.3 Function**

78 The fundamental roles of the SIJ encompass shock absorption, torque conversion, and pelvic
79 stabilization. However, because of its flat shape, the SIJ becomes less stable when subjected to shear
80 loads. The primary source of kinematic support for the connection between the pelvis and the
81 vertebral column provided by the SIJ is rooted in the interconnected ligaments and fascial structures
82 in this area. The primary source of the pelvic ring's structural stability comes from the posterior SIJ
83 complex. This complex is characterized by its unique physical structure and weight-bearing capacity.
84 A suspension bridge-like arrangement of posterior SIJ ligaments, including the ISL, ILL, and PSL,
85 further reinforces it ¹³⁾. Furthermore, the ventral side of the iliopsoas ligament considerably enhances
86 the stability of the SIJ in the sagittal plane, and the ventral side of the ILL significantly improves the
87 stability of the L5-sacral segment ¹¹⁾. Wang and Dumas reported that the transverse segments of both
88 the ASL and PSL resist lateral rotation of the SIJ, with the superior portion of the anterior segment of
89 the posterior ligaments and the inferior segment of the posterior ligaments acting against nutation ¹⁴⁾.
90 These anterior and posterior ligaments together inhibit around 30% of sacral gliding ⁷⁾. The PSL
91 connects to the erector spinae via the posterior layer of the thoracolumbar fascia ⁹⁾; however, the ASL
92 lacks any muscle attachment, with the posterior ligament playing a more substantial role in stability
93 ¹⁵⁾. The smooth, planar articular surfaces of the SIJ allow multidirectional movement, with the robust
94 ISL primarily constraining motion ¹⁶⁾. The role of the ISL is to provide strong joint stability and the
95 axis of rotation for the SIJ ¹⁷⁾. Cadaveric studies indicate that the sacrotuberous ligament has a major

96 role in the kinematic chain linking the pelvis and the vertebral column ⁷⁾. Sacral nutation is restrained
97 by mechanical load exerted on this ligament, an effect that is amplified by the long head of the biceps
98 femoris and the gluteus maximus, both of which anchor to the sacrotuberous ligaments ⁹⁾. The
99 primary role of the sacrospinous ligament is to inhibit rotation of the ilium beyond the sacrum.
100 Dujardin et al. observed a decrease in the stability of the SIJ when the sacrospinous and
101 sacrotuberous ligaments were severed and the ischial tuberosity was compressed ¹⁸⁾. The structural
102 integrity of the SIJ is maintained by a collaborative network of ligaments, which includes the ASL,
103 PSL, ISL, ILL and the sacrotuberous and sacrospinous ligaments.

104

105 **2 Pubic symphysis**

106 **2.1 Bony anatomy and interpubic disc**

107 As described by Becker et al. in their systematic review of the anatomy of the pubic symphysis ¹⁹⁾,
108 the pubic symphysis is essentially a joint that is 10 mm wide and consists of a fibrocartilaginous disc
109 positioned between the articulating surfaces of the pubic bone. These surfaces, which are oblique,
110 oval, and slightly convex in orientation within the sagittal plane, have dimensions averaging 30–35
111 mm in length and 10–12 mm in width and are shielded by a layer of hyaline cartilage measuring 1–3
112 mm in thickness. The interpubic disc, noted for its wedge or Y-shaped axial cross-section with a
113 posterior-directed apex, has a fibrocartilaginous core enveloped by a dense periphery of collagenous
114 tissue. The pubic ligament is connected to this disc ^{19),20)}. The pubic symphysis is almost immobile

115 under the influence of four ligaments.

116 **2.2 Anatomy of the ligaments**

117 **2.2.1 Superior pubic ligament**

118 The superior pubic ligament (SPL) bridges the superior margins of the joint, extending laterally to
119 the pubic tubercles, and it connects to various structures including the interpubic disc, pectineal
120 ligament, line alba, and periosteum of the superior pubic ramus. With average dimensions of 27.7
121 mm in width, 16.0 mm in length, and 3.94 mm in thickness, the SPL does not have significant
122 muscle attachments ²¹⁾.

123 **2.2.2 Inferior pubic ligament**

124 The inferior pubic ligament (IPL), also referred to as the subpubic or arcuate pubic ligament, forms
125 an arch spanning the inferior pubic rami ⁸⁾. As Pieroh et al. describe in their comprehensive
126 description of the pubic ligaments ²¹⁾, the IPL, measuring on average 29.0 mm in width, 14.4 mm in
127 length, and 4.5 mm in thickness, has attachments with the gracilis muscle and partially with the
128 adductor brevis muscle, and it is noted for being the strongest of all the pubic ligaments and thicker
129 than the SPL, anterior pubic ligament (APL), and posterior pubic ligament (PPL).

130 **2.2.3 Anterior pubic ligament**

131 The APL, which measures on average 24.5 mm in width, 30.7 mm in length, and 4.6 mm in thickness
132 ²¹⁾, links the pubic bones at the front and integrates with their peripheral periosteum. It is thickly
133 resistant and has a key role, after the interpubic disc, in maintaining stability of the pubic symphysis.

134 Its deeper layers run more transversely and can blend with the interpubic disc. Its more superficial
135 fibers cross obliquely and interconnect with the tendinous insertions of the rectus abdominis muscle,
136 the oblique abdominal muscles, and the pyramidalis muscle ¹⁹⁾.

137 **2.2.4 Posterior pubic ligament**

138 The PPL, which is positioned on the posterior aspect of the pubic symphysis, tends to consist of a
139 small number of thin fibers. As an independent ligament, it strengthens the pubic periosteum and
140 interconnects with the lateral pubic bladder or puboprostatic ligament. The PPL is not associated
141 with any significant muscle attachments ²¹⁾.

142 **2.3 Function**

143 The pubic symphysis, despite rotating less than 1° during routine activity, is exposed to various
144 forces, including inferior traction, superior compression when standing, and shearing forces during
145 single-leg stance ¹⁹⁾. Its primary function is to aid joint stability rather than joint mobility, which it
146 accomplishes through the reinforcement provided by the four above-mentioned pubic ligaments
147 (SPL, IPL, APL, and PPL). Recent reports highlight the critical role of the IPL and SPL in vertical
148 stabilization and the main contribution of the APL to horizontal stabilization ^{21),22)}. Although the
149 substantial sagittal and coronal dimensions of the APL mean that it can resist high opposing forces in
150 the horizontal plane, and its thickness, muscle connections, and differential layering of fibers make it
151 a key stabilizer ²³⁾, the IPL has a stronger stabilizing effect ^{21),22)}. Indeed, the IPL is the most pivotal
152 ligament for maintaining symphysis stabilization, and it is consistently under tension during daily

153 activities ^{19),22)}. The mechanical strength of the PPL, consisting of only a few thin fibers, remains
154 unclear ²¹⁾.

155

156 **3 Pelvic fracture and ligament stability**

157 Hammer et al. reported that the load distribution during standing was applied to the posterior
158 pelvic ligaments, including the ISL, ILL, ASL, PSL and the sacrospinous and sacrotuberous
159 ligaments. However, the pubic ligaments have a minor effect on overall pelvic motion, primarily
160 facilitating horizontal load transfer at the acetabulum and the ilium ²⁴⁾. The posterior structures,
161 which include the SIJ, afford approximately 60% of pelvic stability ²⁵⁾. The stability of the posterior
162 pelvis should be evaluated accurately and rapidly in patients with pelvic fractures. In terms of
163 fracture classification, the widely used Young-Burgess system categorizes pelvic fractures based on
164 pelvic ring stability and injury mechanism as anterior-posterior compression (APC), lateral
165 compression (LC), or vertical shear injuries. APC and LC injuries are further divided into three
166 stages to indicate their degree of instability, while the extremely unstable vertical shear injury is
167 categorized as a single stage ²⁶⁾.

168 Within the framework of the APC classification, the initial rupture is thought to occur at the
169 symphysis pubis, subsequently extending to the sacrospinous and sacrotuberous ligaments, the ASL,
170 and the ISL, with the final disruption seen in the PSL ²⁷⁾. APC I injuries are marked by disruption at
171 the pubic symphysis or pubic bone but still retain rotational stability of the pelvis, typically showing

172 less than 2.5 cm of symphyseal widening and no findings of posterior instability. In contrast, APC II
173 injuries manifest as rotational instability of the pelvis as a result of disruption of the anterior
174 ligamentous structures and typically have a pubic symphysis diastasis exceeding 2.5 cm and anterior
175 widening of the SIJ. APC III injuries are characterized by disruption of the ISL and PSL, leading to
176 both vertical and rotational instability of the pelvis²⁸⁾. A significant distinction lies at a symphysis
177 pubis diastasis of 2.5 cm, which differentiates a stable pelvis (APC I) from a rotationally unstable
178 pelvis (APC II). This differentiation has substantial clinical implications, considering that APC I
179 injuries do not usually require operative treatment whereas many surgeons opt for operative
180 management of APC II injuries. Upon rupture of the ASL, the average distance of the pubic
181 symphysis is approximately 2.38 cm, which is close to the threshold of 2.5 cm. However, specific
182 measurements across samples have demonstrated variability in the 1.4–4.0 cm range, casting doubt
183 on whether a symphyseal diastasis of 2.5 cm indicates rotation instability²⁹⁾. Stress imaging has
184 recently been performed as an alternative to dilatation of the pubic symphysis to 2.5 cm for accurate
185 diagnosis of APC1 and APC2. Evaluation under anesthesia (EUA), which assesses the stability of the
186 pelvic ring by adding stress, is reported to be important. Using this method, external force is
187 manually applied to the pelvic ring from various directions to evaluate rotational and vertical
188 instability³⁰⁾. This stress examination is performed under fluoroscopy and involves three primary
189 manipulations: adduction and internal rotation of the lower limbs with pressure applied through the
190 greater trochanters; external rotation in the frog-leg position and a lateral force directed at the knees;

191 and finally a push-pull maneuver involving longitudinal traction on one leg and concurrent vertical
192 load on the other leg³⁰. EUA resulted in 27%–50% of APC I injuries being changed to APC II^{30,31},
193 meaning that some APC1 injuries include rupture of the ASL. Furthermore, EUA identified APC2
194 fractures involving a heterogeneous spectrum of injuries. APC2 injuries have traditionally been
195 associated only with external rotational instability. However, when evaluated with EUA, 37% of
196 APC2 injuries also showed rotational instability in the sagittal plane, suggesting a more complex
197 injury pattern³⁰. This finding also suggests that the sacrotuberous ligament, the sacrospinous
198 ligament, and the ASL might be compromised, leading to rotational instability in the axial plane
199^{26,15}). Therefore, Sagi et al. have proposed that the Young-Burgess classification be modified to
200 introduce two subcategories: APC2a for injuries that might be adequately managed with anterior
201 fixation alone and APC2b for injuries that might benefit from both anterior and additional posterior
202 fixation³⁰(Table 1).

203 Moreover, Young and Burgess have further characterized LC injuries according to the degree of
204 posterior ring injury. LC1 is a stable type with pubic and sacral fractures, LC2 is unstable with pubic
205 and iliac wing fractures (crescent fractures), and LC3 is completely unstable and is either LC1 or
206 LC2 with contralateral APC injury (windswept pelvis)²⁶. The distinction between LC1 and LC2
207 injuries plays a crucial role in determining the surgical approach, considering that LC1 fractures
208 represent a heterogeneous spectrum of injuries³². An unstable type of anterior fracture often
209 includes comminuted and/or oblique fractures of the ipsilateral superior pubic ramus and inferior

210 pubic ramus³³). LC1 fractures with an initial sacral displacement of over 10 mm tend to have worse
211 outcomes with non-operative management^{34,35}). However, the absence of these features does not
212 mean that the pelvis is stable. Sagi et al. performed EUA and found that 39% of LC1 injuries
213 demonstrated instability requiring anterior and/or posterior stabilization. These injuries are
214 subdivided into LC1a injuries that are stable and do not require internal fixation and LC1b injuries
215 that may benefit from internal fixation³⁰). Thus, EUA of the pelvis could provide valuable insights
216 about pelvic ring instability and warrants further investigation as a diagnostic tool.

217 However, EUA has some disadvantages. It is costly, requires use and resourcing of the operating
218 room, and carries the risks associated with anesthesia and sedation³³). In contrast, lateral stress
219 radiography (LSR) in the emergency department does not require use of an operating room or
220 anesthesia and reduces the examiner's exposure to radiation^{36,37}). This method also allows for
221 standardization of the force applied to the pelvis and enables formal displacement measurements on
222 radiographs that cannot be easily achieved intraoperatively with fluoroscopy³⁸).

223 LSR and EUA have been shown to have equivalent capability for identifying unstable LC1 pelvic
224 injuries, with sensitivity and specificity of 100% for both modalities³⁷). Another study found that
225 patients with a displacement of 10 mm or more on LSR were more likely to face challenges when
226 mobilizing because of pain, which resulted in delayed surgical intervention, an extended hospital
227 stay, and use of more opioids. The authors of that study recommended that these patients undergo
228 surgery³⁶). Currently, various methods are used to evaluate pelvic instability, including conventional

229 radiography and computed tomography, as well as EUA and LSR.

230 Olson and Matta defined a stable pelvic ring as one that is capable of enduring the physiological
231 forces exerted during protected weight-bearing or during mobilization from bed to chair without any
232 unusual deformation of the pelvis until bone or soft tissue healing is achieved ³⁹⁾. Further research is
233 needed on the ligaments surrounding the SIJ, pelvic floor, and APC and LC pelvic injuries to provide
234 the stable pelvic ring advocated by Olson and Matta.

235

236 **4 Bone mineral density in the pelvis**

237 Osteoporosis, a common condition among older adults, is associated with a heightened risk of
238 fragility fractures ^{40),41)}. The incidence of acetabular fractures has increased the most in patients over
239 60 years of age over the past 25 years, rising 2.4-fold ⁴²⁾. Suneja et al. investigated the incidence of
240 pubic bone fractures in individuals aged 60 years or older using National Electronic Injury
241 Surveillance System data from 2002 to 2019. The incidence of pubic bone fractures in 2019 was
242 found to be approximately 3 times higher than that in 2002 ⁴³⁾. When compared by ethnicity, Asian
243 women had the highest incidence. These are important data for Japan, where the population is aging
244 rapidly and an increase in the number of cases of FFPs is likely.

245 Low-energy traumatic pelvic fractures in older adults have characteristics that are different from
246 those in their younger counterparts. Older patients are often considered non-urgent cases because
247 there is no vascular injury, but there is a history of fragile bones ⁴¹⁾. When performing reconstructive

248 surgery on an osteoporotic pelvis, it is crucial to understand the strength of the bone at the fracture
249 site as the degree of BMD affects the fixation strength of the bone screws used ⁴⁴). Therefore,
250 determining the BMD of the pelvis should be a pivotal step in deciding the treatment plan.

251 Dual-energy X-ray absorptiometry (DEXA) is widely used to measure BMD ⁴⁵), but it is difficult
252 to measure the distribution of pelvic BMD using this method because of the complex shape of the
253 pelvis. DEXA often overestimates BMD as well, because of degenerative changes and vessel
254 calcification ⁴⁶). Recent studies have offered an alternative to DEXA, namely, using Hounsfield units
255 (HU) obtained on computed tomography (CT) scans to measure BMD ^{40,47}). HUs reflect attenuation
256 and the method uses a standardized linear attenuation coefficient. The radiodensity of air is defined
257 as -1,000 HU and that of water as 0 HU at standard temperature and pressure. There is a significant
258 correlation between HU levels and BMD, with HU providing valuable information about the quantity
259 of bone present⁴⁸). For example, according to Gausden et al. ⁴⁷), HU values at the distal radius,
260 thoracic vertebrae, femoral head, femoral neck, and proximal humerus have been used to evaluate
261 BMD in the diagnosis of osteoporosis because of the significant correlation between BMD and HU
262 values at these sites.

263 Wagner et al. published their first investigation of the sacral HU value in 2016. They found that
264 this value was not consistent in the sacrum, with lower values seen in the lateral sacrum and the S2
265 vertebral body ⁴⁰). In 2018, they noted that older patients with sacral fractures had extremely low
266 values of 40 HU in the S1 and 20 HU in the S2 and outside of the sacrum ⁴⁹). These results could be

267 one cause of the high incidence of H-type sacral fractures in older adults. Radley et al. also
268 investigated HU values in the sacrum but in younger adult patients aged 18–50 years and found them
269 to be 320 HU at S1 and 229 HU at S2 ⁵⁰). Furthermore, Thiesen et al. found a difference in the HU
270 values recorded in the sacral vertebral bodies. The HU values in the upper part of S1 and near the
271 anteroposterior cortical bone of S1 were high, as were those in the anterior cortical bone of S2 ²).
272 Inagaki et al. reported HU values for various parts of the pelvic bones, excluding the sacrum ⁵¹).
273 They measured HU values for the pubic bone, the anterior and posterior walls and the roof of the
274 acetabulum, the ischial tuberosity, and the body of the ilium. They also found that HU values were
275 not distributed across the pelvis in a consistent manner, ranging from 120 to 240 HU in the younger
276 group and from 30 to 120 HU in the older group. The HU values for the pelvis were shown to be
277 significantly lower in the older group than in the younger group. Regardless of age, the acetabular
278 roof had the highest values and the anterior pelvis had the lowest. HU values were also found to be
279 higher in the posterior pelvis than in the anterior pelvis ⁵¹) (Table 2). Bredow et al. reported that using
280 pedicle screws in vertebrae of 120 HU or less resulted in screw loosening ⁵²). Given that most HU
281 values in the pelvis of older adults are below 120, screw fixation to the pelvic bone may be
282 inadequate in many cases. This poses a clinical problem for older patients with pelvic fractures,
283 which often require implant fixation that is reliant on screws for anchorage. It is also worth noting
284 that screw fixation through the contralateral cortical bone provides more strength than fixation in
285 cancellous bone ⁵³). Furthermore, spinal surgeons have shifted their approach in osteoporotic bone to

286 guide the trajectory through cortical bone, which increases screw pull-out strength and stability ⁵⁴).

287 Consequently, for improved outcomes, screws should theoretically be anchored through the cortical

288 bone on the opposite side to the fracture. This knowledge is important in preoperative assessment for

289 percutaneous screw fixation, which is a minimally invasive procedure, primarily because the density

290 of cortical and cancellous bones directly influences screw purchase and pull-out strength ⁴⁴).

291 Therefore, understanding the distribution of BMD in the pelvis can improve our understanding of

292 pelvic fracture patterns and their surgical management.

293

294 **Conclusion**

295 This review has outlined the anatomy and function of the ligaments around the pelvis and presented

296 evidence-based discussion of the relationship between fractures of the pelvis and the pelvic

297 ligaments. A more precise understanding of the role that each ligament plays in maintaining stability

298 will further help with the development and selection of surgical interventions for the various pelvic

299 ring injuries. In particular, the extent of injury to the posterior pelvic ligaments should be

300 investigated in depth, because they are primarily responsible for the stability of the pelvis. Changes

301 to the current Young-Burgess classification system to incorporate findings from EUA and LSR would

302 be beneficial, and valuable insights could be afforded by further research on the involvement of

303 ligaments in APC II and other injury patterns.

304 Knowing the distribution of BMD in the pelvis contributes to understanding the different pelvic

305 fracture patterns and their surgical treatment. Such knowledge is also vital as pelvic fractures are
306 becoming increasingly common in older adults, and Asian women are at particular risk. Recent
307 evaluations of BMD of the pelvis using the HU value as an alternative to the DEXA method have
308 revealed low enough HU values in older patients that a screw may pull out. New techniques of screw
309 fixation should therefore be investigated to address this issue.

310

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323

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Table 1 Damaged ligaments, instability, and surgical treatment by injury mechanism

Injury mechanism	Damaged ligaments	Instability	Surgical treatment
APC I	PI	non	non
APC II	II a PI and ASL	Horizontal rotation	Anterior fixation
	II b PI, ASL, STL, and SSp	Horizontal and sagittal rotation	(Anterior) and posterior fixation
APC III	PI, ASL, STL, SSp, ISL, PSL, and ILL	Horizontal, sagittal rotation and vertical force	Anterior and posterior fixation

APC Anterior posterior compression, PI Pubic ligament, ASL Anterior sacroiliac ligament, STL Sacrotuberous ligament, SSp Sacrospinous ligament, ISL Interosseous sacroiliac ligament, PSL Posterior sacroiliac ligament, ILL Iliolumbar ligament

Table 2 HU values at each pelvic region (mean)

	Pubis	AW	Roof	PW	IT	BI
Young men	131	134	235	179	217	219
Older men	35	37	120	89	109	109
Young women	121	118	230	172	210	210
Older women	32	26	118	76	95	92

AW anterior wall, BI body of the ilium, IT ischial tuberosity, Pubis pubic bone, PW posterior wall